



## **Formulation Development with Box-behnken design Study of Ondansetron HCl Ethosome for chemotherapy induced nausea vomiting**

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### **ABSTRACT**

Aim of this work was evaluation of Ethosome by box-behnken design study of Ondansetron HCl Ethosome for physicochemical characterization was carried out by scanning electron microscopy, zeta sizer, particle size analyser and freeze fracture performed. Ethosomes shown a higher % EE greater ability to deliver entrapped drug because of ethonol effect. The optimized batch of Ethosome has zeta potential of -24 mv, vesicle size was found to 242.3nm (PDI = 0.245). *In-vivo* release study performed using Guinea pig skin through Franz's cells for (24 hr). Ethosome shows higher flux by Hyton and chains analysis. Gel prepared by using Carbopol 940 shows pseudoplastic flow. Ondansetron HCl undergoes first-pass metabolism, so its bioavailability may be improved when delivered through transdermal route. The 3-D response plots were constructed from linear model obtained from the regression analysis through Design Expert®. ANOVA on the basis of p-value was found to be less than 0.05 at 95% Confidence limit by student-t test.

**Keywords:** vesicle, box-behnken design, ondansetron HCl, Ethosomes, permeation enhancer.



### **INTRODUCTION**

Cancer Treatment suffer from side effects of nausea and vomiting, To prevent or minimize these side effects of anticancer treatments with 5 HT-3 antagonist such as tropisetron, ondansetron, granisetron and dolasetron, known as serotonin receptor antagonists have been widely administered either parenteral or orally on a daily basis. The transdermal delivery of antiemetic drug is an interesting concept, and seems to be beneficial in a great many patients with chemotherapy induced nausea vomiting[1].

Ondansetron HCl is a potent and selective 5-hydroxytryptamine (5HT-3) receptor antagonist with antiemetic activity indicated for the prevention or treatment of nausea and vomiting associated with cytotoxic chemotherapy radiotherapy and postoperative nausea and vomiting. Ondansetron HCl is rapidly absorbed from the gastrointestinal tract and reaches maximum concentration in serum after approximately 1.6 hr. Ondansetron HCl undergoes first-pass metabolism so its bioavailability may be improved when delivered through transdermal route. So there is a need to develop a transdermal

formulation of Ondansetron HCl which increases patient compliance and non-invasive. The word vesicle' having a biological origin actually means a bubble of liquid within a cell. Technically a vesicle is a small, intracellular, membrane-enclosed sac that stores or transports substances within a living cell[2]. Touitou (1998) discovered and investigated lipid vesicular systems embodying ethanol in relatively high concentration and named them Ethosomes. The basic difference between Liposomes and Ethosomes lies in their composition. The high concentration of ethanol (20-50%) in ethosomal formulation could disturb the skin lipid bilayer organization. Touitou (1998) discovered and investigated lipid vesicular systems embodying ethanol in relatively high concentration and named them Ethosomes. Ethanol acts as a penetration enhancer through the skin. The mechanism of its penetration enhancing effect is well-known. Ethanol penetrates into intercellular lipids and increases the fluidity of cell membrane lipids and decrease the density of lipid multilayer of cell membrane. Increased cell membrane lipid fluidity caused by the ethanol of Ethosomes results increased skin permeability. So the Ethosomes permeates very easily inside the deep skin layers, where it got fused with skin lipids and releases the

drugs into deep layer of skin. Liposome have problem of drug leakage which is overcome by using Ethosome. Stability of vesicle is enhanced by use of the ethanol. Ondansetron HCl BCS -3 drug, so permeation of the vesicle containing Ondansetron HCl enhanced virtue of ethanol effect of ethanol and ethosomal effect of Ethosomes. Literature reveals that no work is reported on ondansetron in gel based vesicular delivery of antiemetic drug is an interesting concept but its clinical use has found limited application due to remarkable barrier properties of the outermost layer of the skin.

Literature also suggests that Ethosomes has better stability than Liposomes, niosomes and more permeation than Liposomes and liquid drug solutions. First time attempt to develop liposomal and ethosomal TDDS for antiemetic drugs for the treatment of chemotherapy induced nausea and vomiting (CINV). Development of sustain release ethosomal and liposomal transdermal gel of ondansetron HCl. Attempt to increase permeation of ondansetron HCl through liposomal and ethosomal based system. Prolonged drug release Reduce dose frequency Improve patient compliance [3]. The animal experiment was approved by Institutional Animal Ethics Committee (IAEC) of Government College of Pharmacy, Aurangabad India (Ref. No. GCPA/IAEC/2012/555- Date: 4/6/2012) and carried out as per the guidelines of the committee.

## MATERIAL AND METHODS

Ondansetron HCl from (Cipla Mumbai), Was a Kind Gift Soya Lecithin from (ResearchLab), Cholesterol from (Dipa Laboratory Chemicals), Carbopol 940 From (Noveon), Ethanol extra pure from (Loba Chemie) All Other Chemicals Was of Analytical grade. Animal guinea pig from Wockhardt. The animal experiments was approved by Institutional Animal Ethics Committee (IAEC) of Government College of Pharmacy, Aurangabad, India (Ref. No. GCPA/IAEC/2012/555- Date: 4/6/2012).

**Preparation of Ethosome:** Preliminary batches of the Ethosomes was prepared by hot method using soya lecithin (10-40mg), ethanol (20-50%) and cholesterol (10 -40 mg) as independent variable. The optimized batch (E5) was selected by Box- Behnken optimization (Table1) and In this method phospholipid soya lecithin is dispersed in water by heating in a water bath at 40°C until a colloidal solution is obtained. In a separate vessel ethanol, propylene glycol 0.5ml and cholesterol are mixed and heated to 40°C. Once both mixtures reach 40°C the organic phase is added to the

aqueous once. The drug initially dissolved in ethanol. The vesicle size of ethosomal formulation can be decreased to the desire extent using Sonication for 15 min. Then formulation is stored under refrigeration at 4°C for 24 hr[4].

**Preparation of Ethosomal Gel:** Ethosomal suspension containing Ondansetron HCl was incorporated into Carbopol 940 (20%w/w) as a gelling agent with constant stirring using a Teflon-coated magnetic bead, and the resulting mixture was then refrigerated at 4°C for 24 hr to obtained a completely hydrated, homogeneous and clear solution[5]. After solution as removed from refrigerator placed at room temperature, until it forms a completely hydrated, homogeneous, and clear gel. (Table2)

## Characterization of Vesicles

**In-vivo Permeation Studies:** The guinea pig skin was mounted on modified franz diffusion cell. In-vivo evaluation of permeation rates of preliminary and optimized ethosomal (E5) was performed respectively and drug solution containing same concentration of Ondansetron HCl through guinea pig skin was studied (As control)[20,21]. At the predetermined sampling intervals, aliquots of 1 ml was withdrawn periodically and replaced with the same volume of fresh receptor fluid (20% PEG). Skin Permeation was studied for 24 hr. Experiments for preliminary batches was performed in triplicate. Drug concentrations was measured by UV-Spectrophotometric method. After the experiment the skin was cut into pieces and kept in 20%v/v (PEG-400) in water for 24hr to determined skin drug content. Then solution was filtered and analyzed by RP-HPLC method[6]. From this amount of drug remain in skin was determined By Hyton and Chien Equation (table 1, 2 and Fig :11)

$$C_n^1 = C_n (Vt/Vt - V_s)(C_n^1 - 1/C_n - 1)$$

## Entrapment Efficiency Determination:

Ethosomal Suspension prepared by hot method Method was further optimized for the entrapment efficiency[7,8,9]. The prepared Ethosomes was kept overnight at 4°C and ultra centrifuged (Megafuge 1.0 R, Heraeus, Hanau, Germany) for 5 hr at 14000 rpm. The free (unentrapped) Ondansetron HCl concentration was determined in the supernatant spectrophotometrically (Shimadzu UV-1601 PC Double Beam, Kyoto, Japan) at  $\lambda_{max}$  310.5nm. The Ondansetron HCl entrapment percentage was calculated from the following formula:

$$EE = [(Q_t - Q_s) / Q_t] * 100$$

**Skin Irritation Studies:** The skin irritation potential of the optimized batch(E5) of Ethosomes

was investigated in guinea pigs [10]. Skin irritation following single application (single insult challenge) was assessed by a visual erythema scoring method (Fig1).

**Vesicle Size and Size Distribution:** Vesicle size of optimized (E5) batch of Ethosomes and was determined using zeta sizer (Beckmann coulter counter) (Fig2 ).

**Microscopic Examination:** Microscopy Olympus® Cx31 Equipped With Magnus Pro.V.3.0. Software of the Optimized E5 Formulations of Ethosomes Revealed the Presence of Ethosomal vesicle.

**Zeta Potential Analysis:** Zeta potential of optimized (E5) batch of Ethosomes was determined using zeta sizer (Beckmann coulter counter) (Fig4). which was initially calibrated according to Beckmann instrument specification [11,12].

**Surface Morphology Evaluation:** Scanning electron microscopy (Jsm-760 Of Philips) Photomicrographs of optimized (E5) batch of Ethosomes vesicle was taken using a scanning electron microscope to study the surface morphology of Vesicle (Fig5).

**Evaluation of Ethosomal Gel Formulations:** The gel formulation containing Ondansetron HCl was evaluated for pH, viscosity, consistency and clarity, drug content uniformity, histopathology (Table3) (Fig8).

**Freeze Fracture Analysis:** Vesicle characterization, the samples, after centrifugation for 30 min at room temperature (Microcentrifuge Ole Dich. NCL Pune), was examined by means of the freeze fracture microscopy technique: samples were impregnated with 30% glycerol and then frozen in partially solidified Freon 22, freeze fractured in a freeze fracture device (-105 8C, 10–6 mm Hg) and replicated by evaporation from a platinum/carbon gun [13]. The replicas were extensively washed with distilled water, picked up onto Formvar-coated grids and examined with a Philips CM 10 transmission electron microscope. (Fig9) .

**Statistical Analysis Optimization:** E5 batch showing max entrapment 74%, flux 27.52(µg/cm<sup>2</sup>/hr), permeability coefficient 2.4(cm/hr) was selected for further studies by box-behnken optimization cube plot. ANOVA on the basis of p-value was found to be less than 0.05 at 95% Confidence limit by student-t test. (Fig 5-10.) Data analysis of factorial batches with statistical software has been very popular,

especially for a small number of factors. For t = 3 factors, the Box-Behnken (BB) design requires only 12 runs, plus a recommended n = 3 center point. Box-Behnken (BB) was used for the study and 3 factors were evaluated variables of study were formula percentage of Ethanol, soya lecithin and Cholesterol. The dependent parameter was drug entrapment, flux and permeation. Experimental design can be defined as the strategy for setting up experiments in such a manner that the information required is obtained as efficiently and precisely as possible. The factorial experimental designs are suitable over traditional optimization in terms of minimum number of experiments and ease in evaluation of statistical significance of independent factors on dependent variables. The factorial design requires lesser efforts than that of traditional optimization methods [14,15].

The factorial design can serve as an essential tool to understand the complexity of mechanisms of pharmaceutical formulations. The polynomial equations are used to evaluate the statistical significance of the obtained responses. An asymmetrical general factorial experimental design was used for study. The ethanol, soya lecithin and cholesterol were independent variables and entrapment (%) flux (ug/cm<sup>2</sup>/hr) and permeability coefficient ug/hr were responses of the study.

$$Y = b_0 + b_1 X_1 + b_2 X_2 + b_{12} X_1 X_2 + b_{11} X_{12} + b_{22} X_{22}$$

Where, Y is the dependent variable,  $b_0$  is the arithmetic mean response of the twelve runs and  $b_i$  ( $b_1, b_2, b_{12}, b_{11}$  and  $b_{22}$ ) is the estimated coefficient for corresponding factor  $X_i$  ( $X_1, X_2, X_{12}, X_{11}$ , and  $X_{22}$ ), which represents the average results of changing one factor at a time from its low to high value. The interaction term ( $X_1 X_2$ ) depicts the changes in the response when two factors are simultaneously changed. The polynomial terms ( $X_{12}$  and  $X_{22}$ ) are included to investigate nonlinearity [19,20]

The final equations in terms of coded values of factors and actual values of factor obtained from ,  
Final Equations for % entrapment in Terms of Coded Factors:

$$\text{Entrapment} = +42.38 + 0.45 * A[1] + 1.44 * A[2] + 6.15 * A[3] - 6.32 * B - 2.86 * C + 6.35 * A[1]B - 4.50 * A[2]B - 1.02 * A[3]B - 1.54 * A[1]C - 3.41 * A[2]C + 4.08 * A[3]C - 3.32 * BC$$

$$(r^2 = 0.0277015)$$

Final Equations for flux in Terms of Coded Factors:

$$\text{Flux} = +14.54 - 9.05 * A[1] - 4.51 * A[2] + 17.23 * A[3] - 4.76 * B + 2.41 * C + 5.90 * A[1]B$$

$$+8.15 * A[2]B - 18.08 * A[3]B - 1.05 * A[1]C - 0.84 * A[2]C + 2.92 * A[3]C + 0.23 * BC$$

$$(r^2 = 0.024947)$$

The percent entrapment and flux of factorial batches is shown in the Tables 14. The summary of response as reported earlier reveals dependence of flux on the concentration ethanol and soya lecithin while cholesterol, another independent variable was found to have overall no significant effect on the entrapment and flux. The effects of variables can be studied by the above equations. The regression coefficient values are used to validate the model fitting [22-23]. The regression coefficient was high indicating the adequate fitting of the quadratic model for response entrapment and flux. The polynomial equations can also be used to draw conclusions considering the magnitude of coefficient and mathematical sign it carries; i.e. positive or negative. If the terms in the equation are positive it contribute positively to the response similarly if the terms is negative it contribute negatively to the response. In the present study positive coefficient of independent factor ethanol showed that it contributes positively to entrapment and flux and leads to enhancement of the drug release at all response points and it is a significant variable in the drug release. However, the negative coefficient of soya lecithin of equations of flux and entrapment indicates significance of independent variable. The analysis of variance study of the data also showed same results revealing the ethanol as significant variable (P value <0.05) at flux, permeability coefficient. As response point and insignificant at entrapment response, while the cholesterol, soya lecithin was insignificant variable at all response point. It again indicates the significance of ethanol in the drug release from the developed formulation of ethosomes.

The 3-D response plots were constructed from linear model obtained from the regression analysis through Design Expert® in which the responses were represented by bars as a function of independent variables as shown in the Figures 9 to 12. The relationship between the response and independent variables can be directly visualized from the response plots. The response and interaction plots used to observe the response's dependence on the input variables to predict this response over the whole of the domain, and possibly also at its periphery. [16,17,18]

## RESULTS

Size of optimized E5 batch of Ethosomes was found in nano range (242.3 nm). It was observed that increase in concentration of ethanol reduces vesicle size which leads to enhancement in

permeation and flux. Polydispersity index of 0.245 indicates that vesicles are monodispersed with distribution of vesicles from 242.3 nm to 349.20 nm range. Vesicle size of optimized Microscopic examination of the optimized Ethosomes batch formulations revealed the presence of vesicles. Zeta potential of optimized Ethosomes E5 batch % entrapment efficiency of optimized was found to be 74%. Flux of optimized Ethosomes E5 batch was found to be 27.52 ( $\mu\text{g}/\text{cm}^2/\text{hr}$ ). Permeability coefficient of optimized Ethosomes E5 batch and flux of was found to be 2.4 ( $\text{cm}/\text{hr}$ ) respectively. Surface morphology analysis performed by using scanning electron microscopy. skin sensitivity test shows no erythema for optimized E5 so suitable for transdermal application. ethosome as better drug delivery for Ondansetron HCl.

## DISCUSSION

In the present study an attempt was made to formulate, optimise and develop ethosomal system of Ondansetron HCl with the aim to have rapid onset of action which will last for prolonged period of time. In preliminary trial batches for preliminary studies two levels of ethanol, two levels of cholesterol and two level of soya lecithin was selected based on entrapment efficiency. Box-behnken design was used for further optimization containing twelve batches. Three independent variables ethanol, soya lecithin and cholesterol was used against entrapment efficiency and flux as dependent variables sows significant effect on formulation. E5 batch showing max entrapment 74%, flux 27.52 ( $\mu\text{g}/\text{cm}^2/\text{hr}$ ), permeability coefficient 2.4( $\text{cm}/\text{hr}$ ) was selected for further studies. Ethosomal gel containing ethosomal suspension (E5) and Carbopol 940 as gelling agent (20 % w/w) was prepared and compared with plain gel containing same drug concentration for in vitro drug release. Comparative *In-vitro* drug release study of plain drug solution, drug in ethosomal suspension form, gel with plain drug and gel with ethosomal suspension was carried out for 24 hours. It was found that cumulative release and flux of ethosomal suspension was more than drug solution containing same drug concentration (less Lag time) and ethosomal gel showed enhanced permeation as compared to plain gel. prepared gels was evaluated for pH, viscosity, consistency and uniformity of content.

## CONCLUSION

Entrapment increases with increase in concentration of ethanol ethosomal gel shows increased in permeation than plain gel containing same drug concentration. Finally, it can be concluded that Ondansetron HCl can be

successfully formulated in gel based ethosomal TDDS which can be used to achieve faster onset of action and the formulation can still prolong the drug delivery for more than 24 hours. However it requires further study on human cadaver skin, in vivo study and establishment if *In-vitro* relations

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Table 1: Ethosomal Box-behnken design

Batch Code	ONDA HCl (mg)	Ethanol(ml)	Soya lecithin (mg)	Propylene glycol (ml)	Cholesterol (mg)	Entrapment (%)	Flux (ug/cm <sup>2</sup> /hr)	Permeability coefficient(x10 <sup>-3</sup> ) (cm/h)
E1	8	3.50	10.00	0.5	10.00	49	1.5	0.014
E2	8	4.00	10.00	0.5	15.00	51	3.82	0.33
E3	8	3.00	10.00	0.5	15.00	41	0.6608	0.0539
E4	8	4.00	15.00	0.5	20.00	44	6.36	0.0564
E5	8	4.00	15.00	0.5	10.00	74	27.52	2.4
E6	8	3.50	20.00	0.5	20.00	47	3.3	0.0294
E7	8	3.50	20.00	0.5	10.00	38	26.93	2.3
E8	8	3.00	15.00	0.5	20.00	42	8.264	0.0733
E9	8	4.00	20.00	0.5	15.00	56	9.1	0.015
E10	8	3.00	20.00	0.5	15.00	50	10.72	0.957
E11	8	3.00	15.00	0.5	10.00	43	12.31	1.093
E12	8	3.50	10.00	0.5	20.00	61	10.71	0.951

\*Box-behnken design

Table2: Ethosomal gel composition

Composition	Ingredients	Quantity
Plain Ondansetron HCl	ONDA HCl	8 (w/w %)
	Carbopol 940	20 (w/w %)
	Water	80 (V/V%)
Ethosomal Gel	Ethosomal suspension (E5 )	80 (V/V%)
	Carbopol 940	20 (w/w %)

Table 3: Ethosomal gel evaluation

Formulation code (E5)	pH	Viscosity (cp)	Clarity	Content Uniformity
Ethosomal gel	5.20	15± 0.26	++	98.01%

\*+ = Poor ++ = Good +++ = Excellent

Table 4: Ethosome parameter evaluation

Sr.no	Parameter	Ethosomes
1	% EE (%)	74
2	Particle size (nm)	242.3
3	Flux(ug/cm <sup>2</sup> /hr)	27.52
4	Permeability coefficient(cm/hr)	2.4
4	P.D	0.245
5	Zeta potential	-14.12

Table 5: Factorial Batches for Ethosome by Box-behnken design

Formulation code	ONDA HCl (mg)	Ethanol(ml)	Soya lecithin (mg)	Propylene glycol (ml)	Cholesterol (mg)
E1	8	3.50	10.00	0.5	10.00
E2	8	4.00	10.00	0.5	15.00
E3	8	3.00	10.00	0.5	15.00
E4	8	4.00	15.00	0.5	20.00
E5	8	4.00	15.00	0.5	10.00
E6	8	3.50	20.00	0.5	20.00
E7	8	3.50	20.00	0.5	10.00
E8	8	3.00	15.00	0.5	20.00
E9	8	4.00	20.00	0.5	15.00
E10	8	3.00	20.00	0.5	15.00
E11	8	3.00	15.00	0.5	10.00
E12	8	3.50	10.00	0.5	20.00

Table6:Summary of Statistical Design

Factor	Names	Units	Type	Subtype	Min	Max	Cod	Values	Std.
A	SOYA LECITHIN	mg	Numeri	Contin	10.00	20.00	1.000=10.00	1.000=20.00	4.08
B	CHOLEST EROL	mg	Numeri	Contin	10.00	20.00	1.000=10.00	1.000=20.00	4.08
C	ETHANOL	ml	Numeri	Contin	3.00	4.00	1.000=3.00	1.000=4.00	0.41

Table7:Summary of Responses

Response	Description	Units	Obs.	Analysis	Min	Max	Mean
Y1	Entrapment	%	12	Polynomial	Min	Max	Mean
Y2	Flux	(ug/cm <sup>2</sup> /hr)	12	Polynomial	38	74	49.6667
Y3	Permeation coefficient	cm/hr	12	Polynomial	0.6608	27.52	10.0996

Table 8 : % EE ANOVA for Response Surface Linear Model

Sum of Source	Square	Mean Df	F Square	P-Value	Prob> F	
Model	327.75	3	109.25	1.11	0.234	Significant
A-SOYA LECITHIN	15.13	1	15.13	0.15	0.188	
B-CHOLESTEROL	12.50	1	12.50	0.13	0.232	
C-ETHANOL	300.13	1	300.13	3.04	0.199	

Table9:Flux ANOVA for Response Surface Linear Model

Sum of Source	Squares	Mean Df	F Square	P-Value	Prob> F	
Model	711.48	6	118.58	4.01	0.0746	significant
A-SOYA LECITHIN	139.10	1	139.10	4.70	0.0823	
B-CHOLESTEROL	196.28	1	196.28	6.63	0.0497	
C-ETHANOL	27.55	1	27.55	0.93	0.0789	

Table 10: Permeation Coefficient ANOVA for Response Surface Linear Model

Sum of Source	Squares	Mean df	F Square	P-Value	Prob> F	
Model	6.66	6	1.11	3.05	0.01206	significant
A-SOYA LECITHIN	0.48	1	0.48	1.31	0.03042	
B-CHOLESTEROL	2.76	1	2.76	7.58	0.0402	
C-ETHANOL	0.049	1	0.049	0.13	0.01294	

Fig 1: Skin Irritation Study


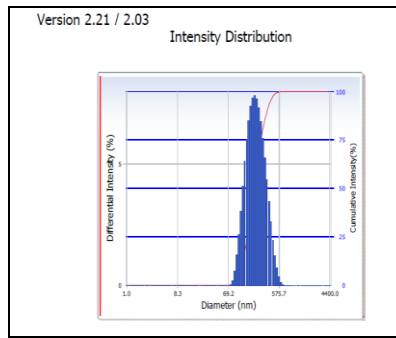
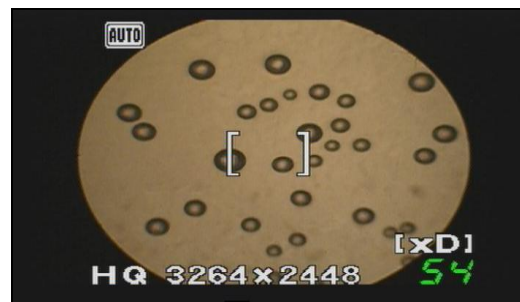
Visual observation	Erythema score	Conclusion	Suitability
 <p>For Ethosome</p>	0	No erythema	Suitable

Fig 2: Vesicle Size of Ethosome E5 batch



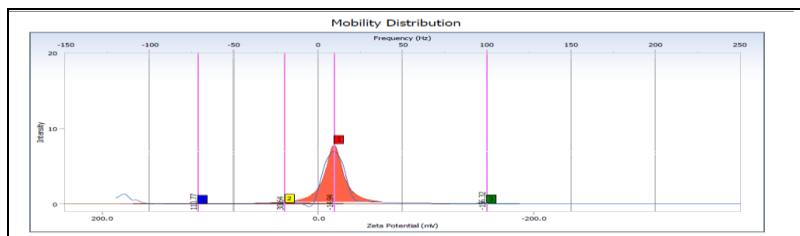
\* E5 batch

Fig 3: Microscopic Examination of Ethosome E5



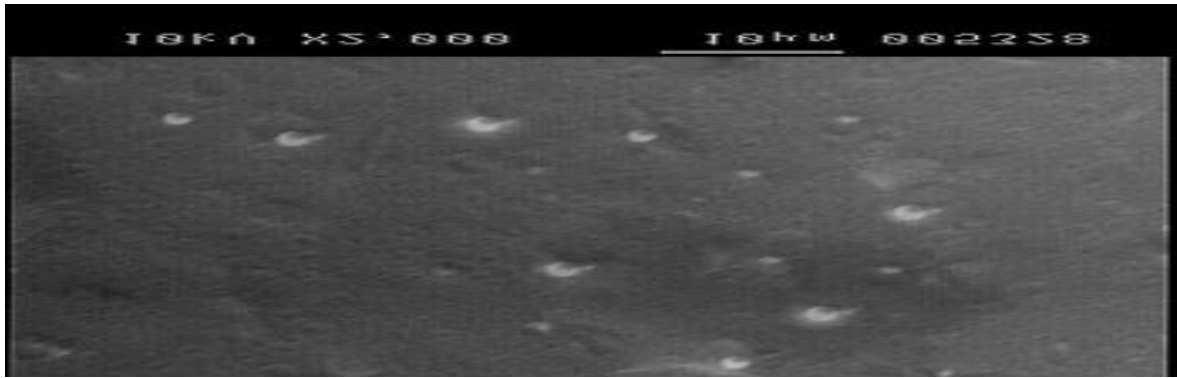
\* Ethosome E5

Fig 4: Zeta Potential Analysis of Ethosome E5



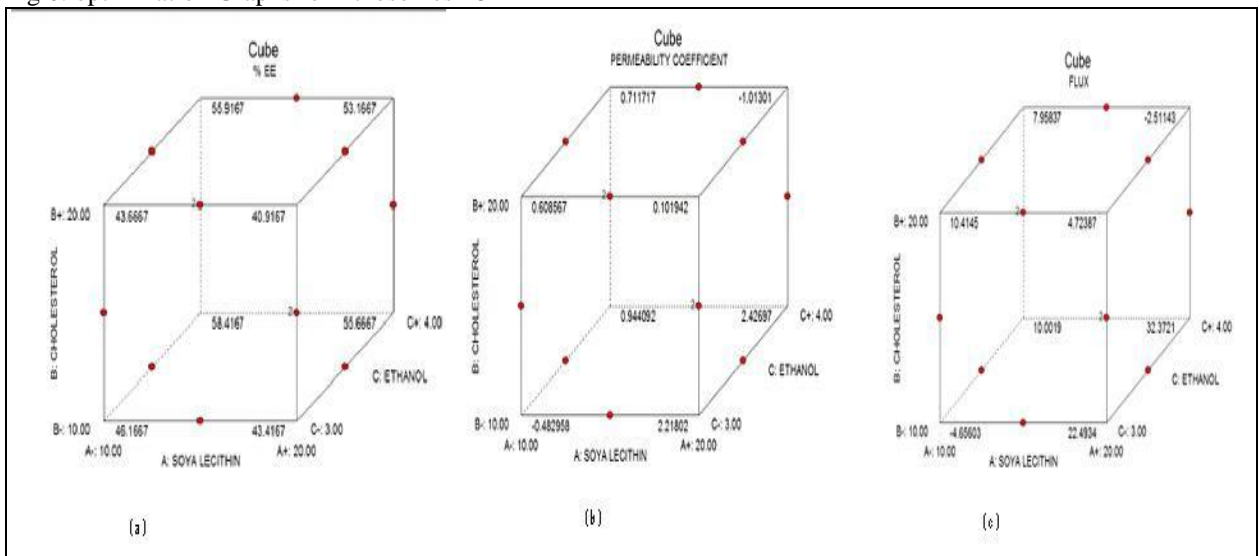
\* Ethosome E5

Fig 5: Surface Morphology Study of Ethosome E5

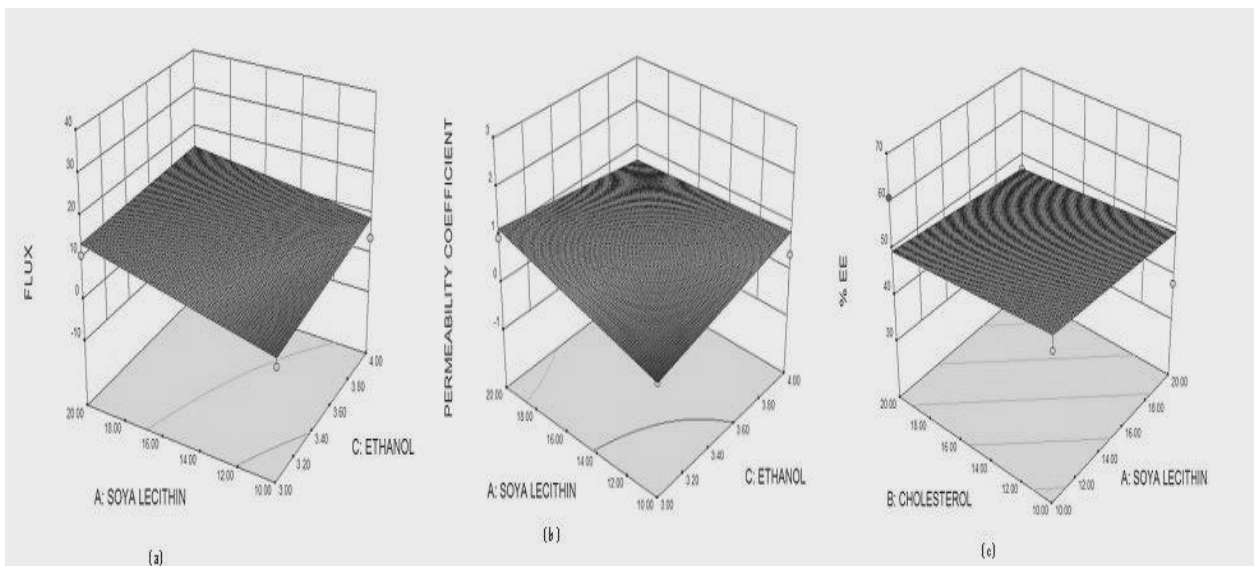


\* Ethosome E5

Fig 6: optimization Graphs for Ethosomes E5



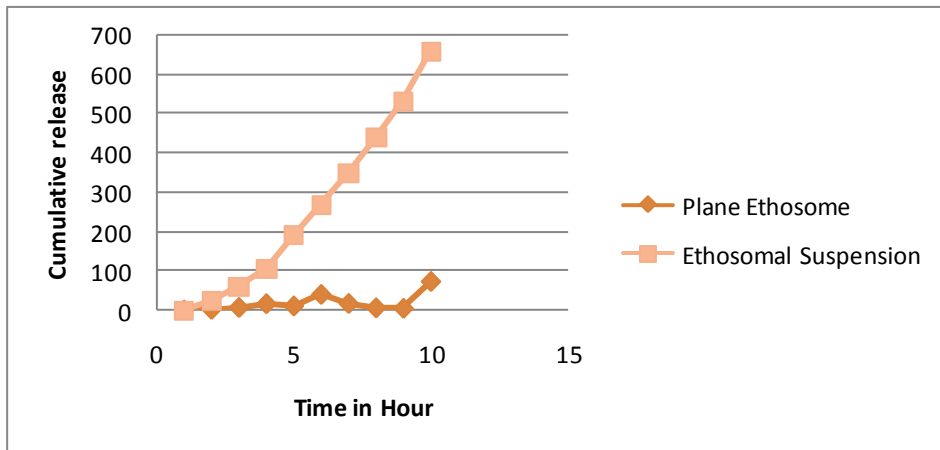
\*cube plot Ethosomes E5



\* response surface plot for Ethosomes E5



Fig 7: cumulative release for Ethosome E5



\* Ethosome E5

Fig8: Histopathology of Guinea pig skin with E5 Ethosome

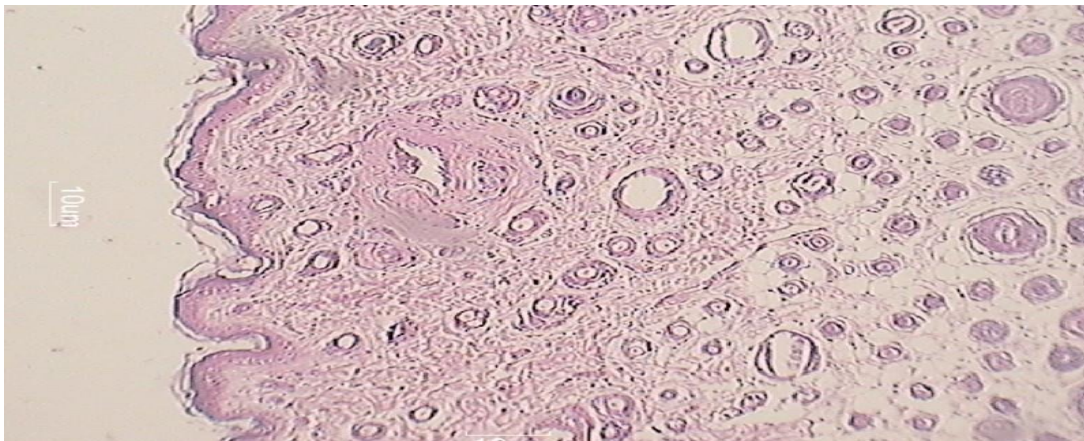


Fig9: Freeze Fracture of E5 Ethosome

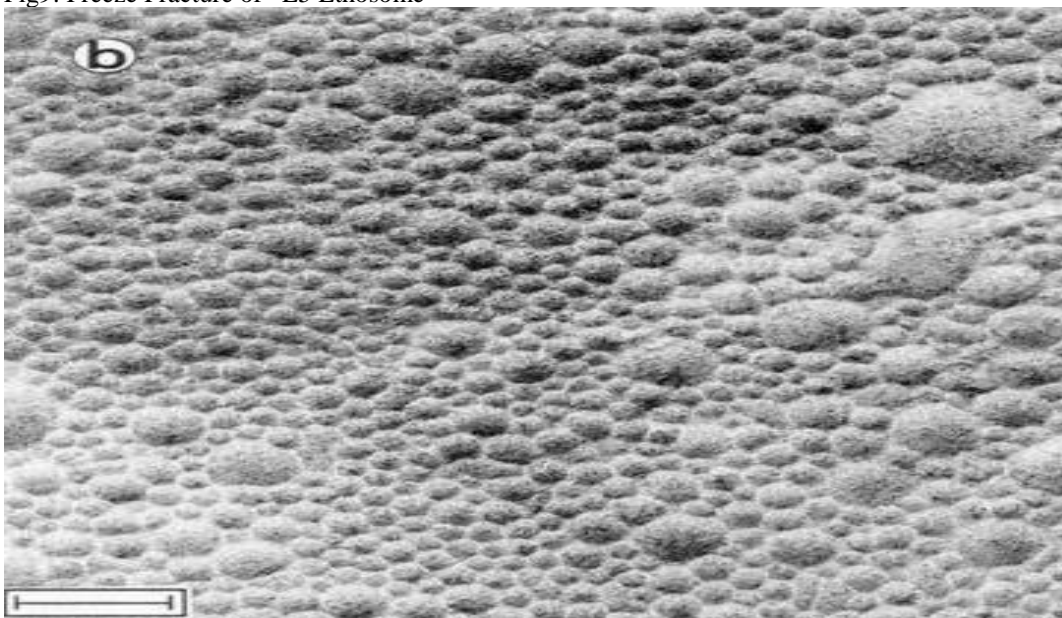


Fig:10 Spreadsheet template for quantification and non-linear regression analysis of data generated from *in vitro* skin permeation study.

A		B		C		D		E		F		G	
<b>In-vitro permeability study</b>													
Sample name		ONDA in NMP 20 mg/ml				Date		07-07-213					
Diffusion cell no.				4									
Diffusion cell volume (ml)		Vr		14									
Surface area exposed (cm <sup>2</sup> )		A		6.15									
donor cell drug conc		Cd		20000									
Sampling volume		Vs		1									
Sampling hr		Measured conc in receptor		Actual drug conc in receptor cell		Drug loss in sampling		Sum total of previous measured samples		Cumulative amt of drug permeated		Cumulative amt of drug permeated per unit area <b>Q/cm<sup>2</sup></b>	
t		Cn		Vr.Cn		Vs.Cn		Vs Σ Cm		Q			
1		0.2762		3.8668		0.2762		0.2762		3.8668			0.6287
2		1.3694		19.1716		1.3694		1.6456		20.8172			3.3849
3		3.0482		42.6748		3.0482		4.6938		47.3686			7.7022
6		14.211		226.9540		16.2110		20.9048		247.8588			40.3022
12		54.0327		765.4578		54.0327		74.9375		831.3953			135.1862
24		119.7569		1676.5966		119.7569		134.6944		1871.2910		304.2750	
48		222.2222		3111.1108		222.2222		416.9166		3528.0274		573.6630	
Slope (Permeation flux) (micgm/cm2/hr)		J		12.36075		Diffusion parameter D'		0.0278					
Intercept (Lag time)		L t		6.00000		Partition Parameter K'		0.0226					
Permeability coefficient		P		0.0063									
<b>NONLINEAR REGRESSION ANALYSIS</b>													
Time		Amt permeated/ unit area		Model equation		UpperCI		Lower CI		D'		0.0918	
1		0.6287		-10.3054		26.9268		47.5376		K'			0.0011
2		3.3849		2.3156		39.5478		34.9166		Mean of y			152.1632
3		7.7022		14.9366		52.1688		22.2956		df			5.0000
6		40.3022		52.7996		90.0318		15.5674		SE of y			14.4840
12		135.1862		128.5256		165.7579		11.2934		R <sup>2</sup>			0.9962
24		304.2750		279.9776		317.2099		212.7454		Critical t			2.5706
48		573.6630		582.8817		620.1139		345.6494		CI		37.2322	
cell C10 formula =		\$C\$4*B10				Copy to cell C16						Press Ctrl+Shift+Enter Press Ctrl+Shift+Enter	
cell D10 formula =		\$C\$7*B10				Copy to cell D16							
cell E10 formula =		D10											
cell E11 formula =		D11+E10				Copy to cell E16							
cell F10 formula =		C10											
cell F11 formula =		C11+E11				Copy to cell F16							
cell G10 formula =		F10/\$C\$5				Copy to cell G16							
cell B31 formula =		SLOPE(Linear portion of graph)											
cell B32 formula =		INTERCEPT(Linear portion of graph)											
cell D31 formula =		(1/(6*\$B\$32))											
cell B33 formula =		(\$B\$31/\$C\$6)											
cell D32 formula =		(\$B\$33/\$D\$31)											
cell C37 formula =		(\$C\$5*\$G\$37*\$C\$6)*(((\$G\$36*A37)-(1/6))				Copy to cell C43							
cell G38 formula =		AVERAGE(B37:B43)											
cell G39 formula =		COUNT(B37:B43)-COUNT(G36:G37)											
cell G40 formula =		SORT(SUM((B37:B43-C37:C43)^2)/\$G\$39))											
cell G41 formula =		1-SUM((B37:B43-C37:C43)^2)/SUM((B37:B43-\$G\$38)^2											
cell G42 formula =		TINV(0.05,\$G\$39)											
cell G43 formula =		G42*G40											
cell D37 formula =		C37+\$G\$43				Copy to cell D43							
cell E37 formula =		C37-\$G\$43				Copy to cell E43							

REFERENCES

1. Espirito J, Chase J. *Cancer Chemotherapy Comprehensive Pharmacy Review*, 5<sup>th</sup> edition, Lippincotts Williams & Wilkins, **2004**, [1096-1115].
2. Graves T. Emesis as complication of cancer chemotherapy: Pathophysiology, importance and treatment, *Pharmacotherapy*, **1992**, 12, [337-345].
3. Bokemeyer C, Hartmann JT., Oral and Gastrointestinal Toxicity In: Lipp HP. *Anticancer drug Toxicity: Prevention, Management and Clinical Pharmacokinetics*, Marcel Dekker Inc., **1999**, [ 235].
4. Del FA, Roila F, Tonato M. Reducing chemotherapy-induced nausea and vomiting: current perspective and future possibilities, *Drug Safety*, **1993**, 9, [410-428].
5. Miller AD, Leslie RA, The area prostrema and vomiting, *Front Neuroendocrinol.*, **1994**, 15 (4), [ 301-320].
6. National Comprehensive Cancer Network (NCCN), *Nausea and Vomiting: Treatment Guidelines for Patients with Cancer*, Version III, American Cancer Society, **2005**, [ 7].
7. Marek C. Continuing Education: Antiemetic therapy in patients receiving cancer chemotherapy, *Oncol. Nursing Forum*, **2003**, 30 (2), [ 1-18].
8. Sweetman SC. *Martindale: The complete drug reference*, 35<sup>th</sup> edition, Pharmaceutical press, **2007**, [1526-1602].
9. Gralla RJ, Osaba D, Kris MG, Recommendations for the use of antiemetics: evidence based, clinical practice guidelines, American society of Clinical Oncology, *J. Clin. Oncol.*, **1999**, 17 (9), [2971-2994].
10. Greene RJ, Harris ND. *Pathology and therapeutics for pharmacists- A basis for clinical pharmacy practice*, 2<sup>nd</sup> edition, Pharmaceutical Press, **2000**, [332].
11. Maibach HI, Shah VP., *Topical Drug Bioavailability, Bioequivalence and Penetration*, Plenum Press, **1993**, [ 19].
12. Beverley JT, Barrie CF. The transdermal revolution, *Drug Discovery Today*, **2004**, 9(16), [697-703].
13. Wang B, Siahaan T, Soltero RA. *Drug Delivery: Principles and Applications*, John Wiley & sons, **2005**, [69].
14. Selzer T, Botsem P, Kindel H, Hoffman G. Transdermal therapeutic system for the delivery of Lerisetron, **2001**, PCT WO 01/74338 A1.
15. Franz JB. Composition for the transdermal delivery of Lerisetron, **2000**, US006136807A.
16. Stinchcomb AL, Nalluri BN, Transdermal delivery of Cannabinoids, **2002**, US2002/0111377 A1.
17. Murthy RB, Chowdhary DK. Pharmaceutical composition containing Tetrahydrocannabinol and a transdermal/transcutaneous delivery method thereof, **2003**, US6503532 B1.
18. Gonyer, Heck. Transdermal delivery of dexamethasone and Promethazine, 2008, WO 2008/103852 A1.
19. Ghosh TK, Jasti BR, Abraham W. *Transdermal and topical drug delivery systems ,Theory and practice of contemporary pharmaceuticals*, CRC press, 2005, [435-436].
20. Shina S, Kima H, Oha I, Chob C, Yang K. Development of tretinoin gels for enhanced transdermal delivery, *Eur. J. Pharm. Bio.*, **2005**, 60, [67-71].
21. Jain NK. *Controlled and Novel Drug Delivery*, CBC Publishers and Distributers, New delhi, **1997**, [100].
22. Gennaro A. *Remington: The science and practice of pharmacy*; Lippincott Williams and Wilkins, New York, **2001**, [ 842].
23. Banga A. *electrically assisted transdermal and topical drug delivery*, Taylor and Francis, **1998**, [1-13].